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Syringe Pump With Nearly Empty Indicator Based on Microcontroller Atmega328 Lely Erica Putri, M. Ridha Mak'ruf, Abd. Kholiq Department of Electromedical Engineering PoltekkesKemenkes, Surabaya Jl. Pucang Jajar Timur No. 10, Surabaya, 60245, Indonesia lelyericaputri@gmail.com, m.reedha@gmail.com, kawullah@gmail.com Abstract— Syringe Pump is a tool used to give liquid medicine or food liquid into the patient's body in a certain amount and within a certain period of time on a regular basis. The purpose of this study is to facilitate the monitoring of fluid in the syringe so that the hose is not installed continuously when the liquid has run out. The

circuit consists of an Atmega328 microcontroller, a motor driver, and an optocoupler sensor. Setting the syringe, volume and flowrate are done at the beginning. To insert liquid, the motor must be run by the way the settings have been done and press the start button. Tools need supply from PLN grids. Calibration is done using IDA 4 Plus. This tool is equipped with the addition of alarms nearly empty and the bolus button. From the measurements taken, at the 20 ml syringe, the biggest error occurred at the 5 ml volume point of 0.4% and at the 50 ml syringe the biggest error occurred at the 5 ml volume point of 0.280%. This module can be used according to its function because the % error is still below the $\pm 5\%$ standard.

Keywords—Syringe Pump; Driver Motor; Optocoupler I.

INTRODUCTION

The hospital is a very complex system so it is difficult to control every patient. For patients who need extra and intensive treatment, we need a tool that can control the dosage of drug use volume and flowrate to be injected. Flowrate is the amount of fluid flowing per unit time. The medical device that can automatically inject is a syringe pump. In this case, the nurse only gives input on the tool in the form of the volume of drugs needed and flowrate which is conditioned by the patient's needs. A syringe pump is one of the electromedical equipment that functions to insert the liquid medicine into the patient's body within a certain period of time on a regular basis. A syringe pump is a drug that is inserted in a syringe that is inserted into the body through veins. In the syringe itself, there are several parameters, namely the amount of volume and flow rate. In this case, the nurse only gives input to the tool in the form of the volume of drug needed and flowrate which is conditioned by the patient's need to get the volume of drug per hour (ml/hour)[1] [2]. In some cases of patients such as hypertension before surgery, heart disease, and neurological diseases, the administration of liquid drugs must be carried out intensively, namely, the fluid volume of the drug must be at a constant flow rate. In patients with critical conditions, intensive care is needed in order to avoid fluid imbalance in the body[3]. The drug fluid is inserted into the patient's body through intravenous injection for a long duration with flowrate adjusted to the right level so that a syringe can be programmed automatically. A syringe pump is a medical device that is used to inject liquid drugs continuously with therapeutic and diagnostic purposes[4] [5]. In this case, the module to be created is equipped with an alarm nearly empty. This alarm is an indication of the volume of drugs approaching the syringe pump. This alarm is a marker that the volume will run out so the nurse can approach the device so that the hose is not installed continuously when the volume has run out. This nearly empty alarm will sound 3 minutes before the volume of liquid runs out. The alarm will sound for the last 3 minutes and turn off when the volume is up [6]. In 2006 Siti Maghfiroh conducted research entitled "Syringe Pump based on the ATmega89S51 microcontroller". The advantages of this research are the mechanics used to design it themselves. The disadvantage of this study is that it still uses 1 syringe, which is 50 ml size and uses 10 ml/hour flow rate. In 2011 Sheindy Chandra Kusumawati conducted a study entitled "Dual Spuit Syringe Pump". The advantage of this study is to use 2 kinds of syringe sizes of 20 ml and 50 ml and the flow rate used is 10 ml/hour and 20 ml/hour. The disadvantage of this study is that the error value is still very high so that at 5 ml volume it cannot be used. In 2013 Meinar Dwi Anggraeni conducted research entitled "Portable Syringe Pump". The advantage of this research is that it is portable, no longer requires PLN grids but uses batteries. The disadvantage of this study is that battery life lasts only 1 hour. In 2018 Faizatul Rosyidah conducted a study entitled "Monitoring of Drip Infuse Pump and Syringe Pump". The advantage of this research is that it can monitor the fluid injected through a PC. The disadvantage of this study is the absence of additional boluses and safety indicators in patients. Based on the

identification of the problems above, the author intends to design a syringe pump equipped with nearly [Journal of Electronics, Electromedical, and Medical Informatics \(JEEEMI\) 25](#) empty based atmega328 microcontroller which can be used as a reminder 3 minutes before the liquid runs out so that the hose is not continuously attached to the patient's body when the liquid has run out. [II. MATERIALS AND METHODS A. Experimental Setup This study uses](#) two syringes of size 20ml and 50ml. The volume used starts from 5ml to 50ml with an increase of every 5ml and with 4 different types of flowrate at different speeds. Retrieval of the data is done 5 times. 1) Materials and Tool This study uses an original stepper motor from a B Broun syringe to drive fluid in the syringe and optocoupler sensor to calculate motor rotation. The components used include Atmega328 as a microcontroller, a motor driver to drive the motor and a 4 x 16 LCD [as a display.](#) 2) [Experiment In this study,](#) the measurement of [the](#) motor driver circuit was carried out by using an oscilloscope. This measurement aims to see the output of the motor driver with a different flowrate setting so that the different frequency and period values are obtained for each flow rate. The researcher also conducted data retrieval using an IDA 4 Plus calibrated tool to calibrate the volume and flowrate made by the researcher. B. The Diagram Block When the device is turned on the MCU or microcontroller will wait for the command from the settings to run the motor. The settings needed are syringe settings, volume settings, and flowrate settings. All settings will be displayed on the display. The microcontroller will instruct the motor driver to run the motor and push the syringe. The optocoupler circuit here serves to calculate the number of turns of the motor that is used as a reference for the microcontroller input and convert it to ml units to be used to calculate the remaining volume. If 3 minutes before the liquid runs out, the buzzer will ring. When the volume runs out the motor will stop working. Motor Driver Program Motor Sruit Setting Push Button Mikrokontroler Nearly Empty Volume Habis Display Fig. 1. Diagram Block Motor Circuit Counter (Opto coupler) Buzzer Buzzer Begin Initialization On Arduino Setting Sruit, Volume, Flow rate Display Setting Sruit, Volume, Flowrate Enter Motor ON NO Empty Volume NO Show The Rest Of The Volume YES Buzzer ON Nearly Empty Motor OFF YES End Buzzer ON Fig. 2. [Flowchart of the](#) Arduino [Program C. The Flowchart](#) When [the](#) tool [is](#) turned [on the](#) tool initializes it first. After setting the syringe, volume (ml) and flow rate (ml/hour). The results of the settings [will be displayed on the display,](#) then [press start to](#) run [the](#) motor. After that, [the](#) display will display the remaining volume. If the volume approaches nearly empty, then the buzzer will sound. The buzzer will sound 3 minutes before the volume runs out. The buzzer will sound until the volume has run out and the motor will stop working. D. The Analog Circuit The important part of this tool is the analog circuit illustrated in Fig. 3 (optocoupler), Fig. 4 (motor driver). 1) Optocoupler Fig. 3. Optocoupler Circuit The Optocoupler circuit is shown in Fig. 3 consists of The microcontroller circuit shown in fig.5 is used for transistor photos and infrared. Where when there is an object processing data from the motor driver and optocoupler that is between the sensor gap, the transmitted light cannot be outputs. The optocoupler sensor will enter the pin A0 and the received by the receiving party, so that it produces an output motor driver enters the digital pin 2. voltage whose value is close to VCC which is 5V. If there is no object between the sensor slits it will produce an output III. RESULTS voltage whose value is close to 0V. In this study, trials have been carried out on the tool 2) Motor Driver directly by using syringes 2 different sizes and the results set with the output will be seen in the measuring cup. The researcher also took measurements using the syringe pump calibrator, IDA 4 Plus as a comparison. Fig. 4. Motor Driver Circuit The motor driver circuit shown in Fig. 4 uses the ULN 2003 IC. There are 4 inputs that will be connected to the microcontroller circuit and 4 outputs to enter the

stepper motor. This driver serves to drive the motorbike driver using logic inputs with varying loop settings as needed. This driver Fig. 6. Module Design will switch the output logic of the microcontroller to the motor pin alternately.

1) The Modul Design The photo section of the microcontroller and motor driver of this tool is shown in Fig. 6. Parts of the microcontroller which consists of Atmega328 as a system regulator, crystal 16,000 MHz which functions as an external clock to carry out the functions of the microcontroller. In the motor driver, there is a ULN2003 IC that drives the motor so the motor can rotate.

2) The Listing Program for Arduino Arduino program listing consists of the initial setting program (selection of syringes, volume settings, and flowrate settings) shown in Program Listing 1, the program for setting the flowrate value shown in Program Listing 2, and the program calculating the remaining volume shown in Program Listing 3. Listing program 1. Program to Initial Setting

```
void settingsyringe() {
  tbup = digitalRead(up);
  tbdn = digitalRead(down);
  if (tbup == HIGH) {delay(500); pilihan = pilihan + 1;}
  if (tbdn == HIGH) {delay(500); pilihan = pilihan - 1;}
  if (pilihan == 1) {syringe=20;}
  if (pilihan == 2) {syringe=50;}
  if (pilihan > 2) {pilihan = 1;}
  if (pilihan < 1) {pilihan = 2;}
}
```

Fig. 5. Microcontroller

3) Measurement of Output Circuit of Motor Driver on void settingvolume()

```
{delay(500); volume = volume + 5;}
if (tbdn == HIGH) {delay(500); volume = volume - 5;}
if (volume > 50) {volume = 0;}
if (volume < 0) {volume = 50;}
void settingflowrate() {
  delay(500);
  flowrate = flowrate + 5;
  if (tbdn == HIGH) {delay(500); flowrate = flowrate - 5;}
}
```

Fig. 7. The output from ATmega328 pin at a flow rate of 5 ml/hour

```
if (flowrate > 20) {flowrate = 0;}
if (flowrate < 0) can see an output with an amplitude of 4.88V, a 50% duty cycle {flowrate = 20;}
cycle with a frequency of 266.7 MHz with a period of 3,750 s. }
TON results obtained at 50% and TOFF results obtained at 50%.
In the condition of the TON, the motor driver gets high Listing Program 2.
Program to Setting the Flowrate Value logic, the motor will work while in the TOFF condition the motor driver gets a low logic, and the motor will stop.
if (flowrate == 5 && syringe == 20) {kecepatan = 2.95;}
if (flowrate == 5 && syringe == 50) {kecepatan = 1.2;}
if (flowrate == 10 && syringe == 20) {kecepatan = 4.2;}
if (flowrate == 10 && syringe == 50) {kecepatan = 2.55;}
if (flowrate == 15 && syringe == 20) {kecepatan = 6;}
if (flowrate == 15 && syringe == 50) {kecepatan = 3.75;}
Based on the picture above, the ATmega 328 pin 4 output if (flowrate == 20 && syringe == 20) can see an output with an amplitude of 4.88V, a duty cycle of {kecepatan = 8;} 50.03% with a frequency of 533.3 MHz with a period of 1,875 if (flowrate == 20 && syringe == 50) s. The TON results obtained were 50.03% and the TOFF {kecepatan = 4.48;} results were obtained at 49.97%.
In the condition of the TON, } the motor driver gets high logic, the motor will work while in the TOFF condition the motor driver gets a low logic, and the Listing Program 3.
Program to count the remaining volume motor will stop. void volumesisa() {
  float flowrate2 = flowrate;
  volume1 = volume/10;
  volumenearly = (flowrate2/60)*3;
  sisavolume = (volume1 - volumekeluar)*10;
  if (sisavolume <= volumenearly) {
    lcd.setCursor(-3, 3);
    lcd.print("NEARLY EMPTY");
  }
  digitalWrite(buzer, HIGH);}
Based on the picture above at the ATmega 328 pin 4 if (sisavolume < 0.00) output can be seen output with an amplitude of 4.96V, a 50% duty cycle with a frequency of 800 MHz with a period of 1,250 s. TON results obtained at 50% and TOFF results obtained at 50%.
In the condition of the TON, the motor driver gets high logic, the motor will work while in the TOFF condition the motor driver gets a low logic, and the motor will stop. Fig. 10. The output from ATmega328 pin at a flow rate of 20 ml/hour Based on the picture above at the ATmega 328 pin 4 output can be

```

seen output with an amplitude of 4.88V, a 50% duty cycle with a frequency of 1.067 Hz with a period of 937.6 ms. TON results obtained at 50% and TOFF results obtained at 50%. In the condition of the TON, the motor driver gets high logic, the motor will work while in the TOFF condition the motor driver gets a low logic, and the motor will stop. 4) The Error of Volume (ml) Value The volume measurement results in each set are measured by the IDA 4 Plus tool. The error value is shown [in Table I. TABLE I. THE ERROR OF MEASUREMENT FOR VOLUME SETTINGS 20 ML SPUIT](#)

No	Volume (ml)	Error (%)
1	5	2
2	10	3
3	15	4
4	20	5
5	25	6
6	30	7
7	35	8
8	40	9
9	45	10
10	50	0,4
0,4	0,14	0,013
0,030	0,056	0,007
0,040	0,030	0,022
0,052		

TABLE II. THE ERROR OF MEASUREMENT FOR FLOW RATE SETTINGS ON 20 ML SPUIT

No	Flow Rate (ml/hour)	Error (%)
1	5	2
2	10	3
3	15	4
4	20	5
5	75	0,32
0,2	0,05	0,1
0,01		

TABLE III. SPUIT THE ERROR OF MEASUREMENT FOR VOLUME SETTINGS ON 50 ML

No	Volume (ml)	Error (%)
1	5	2
2	10	3
3	15	4
4	20	5
5	25	6
6	30	7
7	35	8
8	40	9
9	45	10
10	50	0,280
0,260	0,067	0,040
0,016	0,00	0,034
0,050	0,009	0,004

TABLE IV. THE SETTINGS ON 20 ML SPUIT ERROR OF MEASUREMENT FOR FLOW RATE

No	Flow Rate (ml/hour)	Error (%)
1	5	2
2	10	3
3	15	4
4	20	5
5	75	0,16
0,10	0,027	0,090
0,061		

IV. DISCUSSION The difference in the selection of flowrate can affect the frequency and period of the microcontroller output signal which can be seen through an oscilloscope. Calculation of the average error with a 20ml syringe is = 0.09% and with a 50ml syringe value = 0.085%. Errors can be caused because the mechanical motor used is less stable, the voltage at the supply decreases and the reading resolution is high. On ECRI's provisions about the maximum permissible errors in the syringe pump which is equal to 5%, so the syringe pump module is equipped with nearly empty microcontroller ATmega 328 worthy of use.

V. CONCLUSION Based on the [results of the discussion and the purpose of making the module it can be concluded that](#) after volume measurement using a 20 ml syringe, the smallest error occurred at 30 ml volume point of 0.007% and the biggest error occurred at 5 ml volume point of 0.4%. Volume measurement using 50 ml syringe, the smallest error occurred at 30ml volume point of 0% and the biggest error occurred at 5ml volume point of 0.280%. Software to run a minimum series of microcontroller systems in running well so that it can run the tool according to the settings. The tool can work well because the biggest error value is 0.4% while the maximum error allowed is 5%. References [1] K. K. Tulungagung, "ADLN Perpustakaan Universitas Airlangga 1," pp. 1-8, 2017. [2] Y. C. Yu, "Automatic monitoring of the infusion system in a rotary heart assist device," in Proceedings of the IEEE Annual Northeast Bioengineering Conference, NEBEC, 2003, vol. 2003-Janua, pp. 116- 117. [3] F. R. Halim, Suwandi, and A. Suhendi, "Rancang Bangun Syringe Pump menggunakan Motor Stepper Berbasis Arduino," e-Proceeding Eng., vol. 3, no. 2, pp. 2078-2085, 2016. [4] I. Saidi, L. ElAmraoui, and M. Benrejeb, "Multi-physics modeling of a linear tubular step actuator," Int. Rev. Model. Simulations, vol. 3, no. 6, pp. 1202-1208, 2010. [5] G. Cocha, J. Rapallini, O. Rodriguez, C. Amorena, H. Mazzeo, and C. E. Drattellis, "Intelligent Insulin Pump Design," in Congreso Argentino de Ciencias de la Informatica y Desarrollos de Investigacion, CACIDI 2018, 2018, pp. 7-10. [6] M. Deepalakshmi and R. Jayaparvathy, "Design and implementation of a lowcost Integrated Insulin Infusion system," in 2016 International Conference on Computation of Power, Energy, Information and Communication, ICCPEIC 2016, 2016, pp. 25-32. [Journal of Electronics, Electromedical, and Medical Informatics \(JEEEMI\) Vol. 1, No. 2, October 2019, pp. 25-30 DOI: 10.35882/jeeemi.v1i2. 5 ISSN:2656-8632](#) [Journal of Electronics, Electromedical, and Medical Informatics \(JEEEMI\) Vol. 1, No. 2, October 2019, pp. 25-30 DOI: 10.35882/jeeemi.v1i2. 5 ISSN:2656-8632](#) [Journal of Electronics, Electromedical, and Medical Informatics \(JEEEMI\) Vol. 1, No. 2, October 2019, pp. 25-30 DOI: 10.35882/jeeemi.v1i2. 5 ISSN:2656-8632](#)

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