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Simple and Low Cost Design of Infusion Device Analyzer Based on Arduino
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¹Department [of Medical Electronics Engineering Technology Politeknik Kesehatan Kementerian Kesehatan Surabaya Jl. Pucang Jajar Timur No. 10, Surabaya \(60282\), Indonesia](#) ²University of Punjab [,Department of Electrical Engineering Information Technology, Lahore, Pakistan](#) North Underpass, Quaid-i-Azam Campus, Lahore, Punjab 54590, Pakistan [E-mail: nikmatulj10@gmail.com](#) [Article Info](#) [Abstract](#) [History Articles](#): In the medical world, patient safety is a top priority. The number of workloads and frequency of use Receive Mei 15, 2020 in the long term will affect the accuracy and precision of the equipment. Therefore calibration is needed, Revised August 10, 2020 namely the measurement activities to determine the truth of the appointment value of measuring Received August 30, 2020 instruments and measuring materials [based on the standards of the Minister of Health](#) Regulation No. 54/2015. The [purpose of this study is to design](#) an infusion [device](#) analyzer [to](#) measure [the](#) flowrate Keywords: parameter using the Arduino microcontroller. The main advantage of this study is that the system can Calibration display three calibration results in one measurement at the same setting. The results of the calibration Flowrate will determine the feasibility of an infusion pump or a syringe pump. This study uses the flow rate formula, which is applied to the water level system to obtain the calibration results. The infrared Microcontroller photodiode sensor will detect the flow of water in the chamber that comes from the infusion or syringe Water Level pump. Furthermore, the [sensor output will be processed](#) by [the microcontroller](#), and [the](#) reading results are displayed on the liquid crystal display. The average measurement at a setting of 10 ml/hour is 9.36 ml/hour, at a setting of 50 ml/hour is 46.64 ml/hour, and at a setting of 100 ml/hour is 96.04 ml/hour. Based on available data, [this tool has an average error value of](#) 5.69%, where the value exceeds the tolerance limit allowed by ECRI, which is $\pm 5\%$. The corresponding author: Syaifudin [Department of Medical Electronics Engineering Technology Politeknik Kesehatan Kementerian Kesehatan Surabaya Jl. Pucang Jajar Timur No. 10, Surabaya \(60282\), Indonesia](#) [E-mail: nyong74@yahoo.com](#) [This jobopen access articles and licensed under Creative Commons Attribution-Non-Commercial 4.0 License International, I. INTRODUCTION](#) In the hospital, intravenous therapy is an important therapy for patients and the most common curing [1][2]. A nurse sets an IV infusion device up according to the doctor's

medical order [1]. Intravenous infusion devices are medical devices that function to deliver fluids, including medicines and nutrients into the patient's circulatory system continuously by controlling the volume or rate of fluid flow precisely and accurately through a needle to treat dehydration due to a disease or after excessive activity by distributing antibiotics or certain [3][4]. These drugs must be given at a certain time and speed of at least 0.5 ml/ hour. This level cannot be reached accurately with normal intravenous infusion [5]. The medical devices commonly used for administering such fluids are infusion pumps and syringe pumps. Both devices have an important function, which is an alarm system that will sound if the infusion speed exceeds or is lower than a certain range. Therefore, the detection and calculation of speed are related to the accuracy of the infusion device [2]. The infusion pump and syringe pump are very efficient, fast, and precise methods [6]. The advantage of using an infusion pump or syringe pump is that medical personnel do not need to count the number of drops or volumes manually because in both devices there are already settings for flow rate and volume that will automatically enter the liquid at a constant speed and for a certain time. In the health industry, be it a hospital or medical equipment factory, patient safety is a top priority. Intravenous therapy can cause several problems such as air embolism, excess fluid, and changes in the droplet rate. Due to changes in droplet rate, lack of infusion causes sub-optimal therapy, dehydration, or metabolic disorders. While excessive infusion can cause speed shock, electrolyte imbalance, high blood pressure, or metabolic disorders [7]. If the flow rate and volume is given to the patient Indonesian Journal of Electronics, Electromedical Engineering and Medical Informatics (IJEEEMI) 80 are not controlled (overdose or fluid flow rate is too high), it can cause hypertension, heart failure, or pulmonary edema and when an occlusion occurs, drugs or nutrients cannot flow into the patient's blood vessels so it becomes inefficient and ineffective [3]. In addition, if air bubbles in the infusion pump or syringe pump enter the patient's venous system can cause serious problems and often fatal. Air bubbles can also spread to the lungs, heart, and brain and cause respiratory failure, stroke, or heart attack [5][8]. This will cause delayed treatment, pain in the patient, or even seriously endanger the physical and mental health of the patient, and medical malpractice occurs beyond repair [9], in the many past reports of functional failure in the syringe pump. Statistical results show that 39% of errors occur when giving drugs, 10% errors appear in pharmacies, and 38% errors are made when infusing drugs, 13% for several other reasons [10]. The use of medical devices with a large workload and the frequency of use, in the long run, will affect the accuracy and accuracy of the device, so it is necessary to re-measure with the aim to minimize errors in the provision of intravenous therapy to patients. Re-measurement in question is to do testing and calibration, especially on medical devices. Calibration is an illumination activity to determine the truth of the appointment value of the measuring instrument and or measuring material [11]. Equipment testing and calibration are useful to ensure the accuracy, effectiveness, and lifetime of the equipment to achieve the highest level of quality control [12]. The instrument used to calibrate the infusion pump, and syringe pump is the Infusion Device Analyzer, which measures the flow rate, volume, and occlusion pressure. The reference used as a guideline when calibrating the infusion pump and syringe pump is ECRI 416- 0595. Allowable flow rate measurements are $\pm 5\%$ for critical patients, $\pm 10\%$ for general patients, and ≤ 20 Psi for occlusion pressure [13]. This tool is very important for the hospital to have so that the equipment is maintained and maintained its quality and accuracy. In this research, the writer wants to propose an infusion device analyzer design with flowrate parameters. The reason the authors chose the flowrate parameter is that these parameters are the main parameters both in the infusion pump and

syringe pump. In doing this research, the authors used previous research as a reference and benchmark for completing research. The existence of previous research makes it easier for writers to formulate theories and concepts and determine systematic steps. Previous research had been conducted by three students of the Electromedical Engineering of Poltekkes Surabaya, namely Yanu Eko Prastiyono (2011) with the title flowrate calibration tool through the volume in microcontroller-based infusion pumps, Adhif Ristiano (2012) with the title pc-based syringe pump calibration tool and Safira Pintasari (2019) with the title design and build infusion pump analyzer. In this study, the authors used the same sensor as the three researchers, namely the infrared photodiode sensor. This research will produce three calibration results in one measurement at the same setting, using a water level system. The water level is used to measure the height of the water from the bottom to the surface. To find out the flow rate at the infusion pump or syringe pump, the writer uses the formula of the water flow rate by determining the volume of water, setting the flow rate on the device measured, and the length of time of measurement. [This article consists of 5 parts.](#) Part I is an introduction, Part II contains the materials and methods to be carried out. [Part III is the results obtained in this study.](#) Part IV is a [discussion of finding](#), and [Part V is a conclusion.](#)

II. MATERIALS AND METHODS

A. Experimental Setup [This study uses](#) the TOP-5300 syringe pump as a tool to be measured. Data collection is carried out sequentially, starting from low to high flow rates. **B. Materials and Tools** [This study uses](#) photodiode and infrared [sensors](#) as flow rate detectors. A two-channel solenoid valve 12VDC was used to close and open water flow. A software Arduino (Version 1.8.11), Arduino Nano V3.0, was used to develop the program of a microcontroller. Finally, an LCD character 2x12, as a display and I2C as a communication between a microcontroller and display. C. [Experiment In this study, researchers measured the output of](#) the circuit using a syringe pump at settings of 10, 50, and 100 ml/hour. Data collection was done 1-time measurement at a flow rate of 10 ml/hour and two times measurement at a flow rate of 50 and 100 ml/hour. D. The Diagram Block [When the appliance is turned on, the power supply will supply voltage to the entire circuit. The sensor will](#) detect the presence or absence of water flowing in the tube chamber from the infusion or syringe pump. The sensor output will enter the [comparator circuit to compare the input voltage of the sensor with the reference voltage.](#) Then the ADC will convert analog data into digital, which is processed by a microcontroller on Arduino Nano. The reading results will be displayed on an LCD character 2004A in the form of a time counting, volume, flow rate, and length of measurement by following the applicable formula. The detailed system is shown in Fig. 1 Push Buttons Photodiode and Infrared Sensors Comparators Programs ARDUINO NANO Display Driver Solenoid Fig. 1. The diagram block of the IDA with Flowrate Parameters E. The [Flowchart](#) [When the device is turned on, the voltage will supply to the entire circuit,](#) and the LCD will initialize. The screen will display the parameter selection. Select the flowrate parameter to measure the flow rate, then press the start button. The solenoid inlet on the device will automatically open, and the sensor will read. The first sensor works as the time counter. When the second sensor is blocked by water, it means that the first measurement time counter is reached and [will be processed by the microcontroller on the](#) Arduino Nano. [The measurement results will be displayed on the](#) screen [in the form of](#) a timer counter, flow rate, volume, and time of measurement. Furthermore, this tool will make the second and third measurements with the same process and settings but with different sensors. When the results of the third measurement appear, the timer will stop, and the solenoid drain will automatically open to drain water. The flow chart [of the proposed method is](#) shown [in Fig. 2](#) Infusion Pump / [Syringe Pump](#) Set Flowrate Begin Initialization Parameter Selection Start Inlet Solenoid Open Read the Sensors No Time Counter

(s) Yes [voltage is higher than the](#) sensor [voltage](#), it indicates [the](#) sensor is not blocked by water. But if the reference [voltage is higher than the](#) sensor [voltage](#), it indicates that [the](#) sensor is blocked by water [14][15]. Fig. 3. Infrared Photodiode and Comparator Circuit 2) Solenoid Driver The solenoid driver circuit functions to regulate the opening and closing of the flow of water that enters the device during measurement. This circuit is connected to the Arduino microcontroller on digital pins 7 and 8 (Fig. 4). Fig. 4. Solenoid Driver Calibration Results Drain Solenoid Open [End Fig. 2. The Flowchart of the Arduino Program F. Circuit 1](#)) Infrared Photodiode and [Comparator The output voltage of the](#) infrared photodiode [will](#) enter [the](#) comparator input (pin -) to be compared with the reference voltage originating from the multivibrator voltage (pin +) (Fig. 3). The sensor has two conditions, namely, [when the sensor is](#) not [blocked](#) by water [and](#) when [blocked by](#) water. When [the](#) sensor [III. RESULT In this study, the](#) instrument [was](#) only [tested](#) using a TOP- 5300 syringe pump without testing it with standard measuring devices. So, it cannot be known whether this tool is suitable for use as a calibrator or not. A. IDA Design [Design tools can be seen in Fig. 5. There is a](#) LCD character 2004A [as](#) [the](#) screen display. It has four pushbuttons consisting of select, enter, start, and reset buttons. At the bottom of the tool there is an inlet as the entrance of liquid from the syringe or infusion pump and Arduino Nano USB connector. On the back, there is a power button and a water drain. Fig. 6 shows the results of a series of solenoid drivers that function to open and close the water flow. In Fig. 7 is the result of a series of infrared photodiode sensors and comparators that function for sensor readings. Fig. 5. Infusion Device Analyzer With Flowrate Parameters Fig. 6. The Results of the [Solenoid Driver Circuit Fig. 7. The Results of the](#) Infrared Photodiode Sensor Circuit and the Comparator B. Listing Program 1) Listing Program For Library and Initialization [#include <Wire.h>](#) [#include <LiquidCrystal I2C.h>](#) [#define BACKLIGHT_PIN 13](#) [LiquidCrystal I2C lcd \(0x27,2,1,0,4,5,6,7,3, POSITIVE\); int pinSolenoid1 = 7;](#) //solenoid inlet [int pinSolenoid2 = 8;](#) //solenoid drain int sensorFlow1, sensorFlow2, sensorFlow3, sensorFlow4 = 0; int timer, v, v1 = 0; int kondisi = 1; int milidetik, jam; int detik = 0; int menit = 0; int down = 0; int enter = 0; int start = 1; int reset = 0; int i = 0; int val = 0; int vol = 0; int kunci = 0; const int pinFlow1 = A1; //start counting const int pinFlow2 = A2; //sensor 1 const int pinFlow3 = A3; //sensor 2 const int pinFlow4 = A6; //sensor 3 [const int sw1 = 3;](#) //down button [const int sw2 = 4;](#) //enter button [const int sw3 = 5;](#) //start button [const int sw4 = 6;](#) //reset button float Flow1, Flow2, Flow3, Flow4, fr1, fr2, fr3, fr4, waktuFlow1, waktuFlow2, waktuFlow3, waktuFlow4 = 0; unsigned long waktusekarang, waktu, waktu2, waktu3, waktu4, reset1, reset2, reset3, reset4, wk1, wk2, wk3, wk4 = 0; 2) Listing Program For Time Counter This time counter program can be run when the required initialization is complete. void waktustart() { unsigned long waktu = millis(); if (waktu - waktusekarang >= 1000) { waktusekarang = millis(); detik++; } if (detik > 59){ menit++; detik = 0; } if (menit > 59){ menit = 0; } lcd.setCursor (19,0); lcd.print (""); if (detik > 9){ lcd.setCursor (18 ,0); [lcd.print](#) (detik); } [if](#) (detik < 10){ [lcd.setCursor](#) (18 ,0); [lcd.print](#) ("0"); [lcd.setCursor](#) (19 ,0); [lcd.print](#) (detik); } [if](#) (menit > 9) { [lcd.setCursor](#) (15 ,0); [lcd.print](#) (menit); } [if](#) (menit < 10) { [lcd.setCursor](#) (15 ,0); [lcd.print](#) ("0"); [lcd.setCursor](#) (16 ,0); [lcd.print](#) (menit); } } 3) Listing Program For Sensor When the flowrate setting is selected, the system will automatically enter the "menu06". The LCD character 2004A display will display volume (V), time counter (T), flowrate results (F1, F2 and F3) and the time for each flowrate result. menu06: while(1) { lcd.clear(); [lcd.setCursor\(0,0\); lcd.print\(" V : mL"\); lcd.setCursor\(0,1\); lcd.print\(" F1: mL/h"\); lcd.setCursor\(0,2\); lcd.print\(" F2: mL/h"\); lcd.setCursor\(0,3\); lcd.print\(" F3: mL/h"\); lcd.setCursor\(13,0\); lcd.print\(" T:"\); delay\(100\); start = digitalRead\(sw3\); reset = digitalRead\(sw4\); if\(start == HIGH\){ lcd.clear\(\); digitalWrite\(7, HIGH\); //solenoid open digitalWrite\(8, LOW\);](#)

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//solenoid closed goto menu03; } } When the start button is pressed, the
inlet solenoid will automatically open and the drain solenoid closes and
the system will enter menu03 which is a sensor reading program. flowrate
sensors enter through analog pins A1, A2, A3 and A6 on Arduino Nano in
the form of analog data and can be written in Arduino as follows:
menu03: while(1) { //=====Start=====
sensorFlow1 = analogRead(A1); //sensor reading float Flow1 =
sensorFlow1*5/1023; if(Flow1<1&&kunci==0) { kunci = 1; timer = 1;
reset1 = millis(); } if(timer == 1) { waktustart(); } if(kunci == 1) {
waktu2=millis()-reset1; } if(kunci == 2) { waktu3=millis()-reset2; }
if(kunci == 3) { waktu4=millis()-reset3; } Based on the measurement
data of the output voltage on the comparator, the authors make the
conditions in the program, namely, if the comparator output voltage is
less than 1 Volt, shows logic 0, and if the output voltage is more than 1
Volt shows logic 1. So, when the sensor is blocked by water, the
microcontroller will get logic 0. However, if the sensor is not blocked by
water, the microcontroller will get logic 1. The sensor reading program
above functions to start the counter. When water gets in the way of the
first sensor, the sensor output voltage will go to the ADC and will be
converted from the sensor value (0-1023 bit) to the voltage value (0 -
5V), the microcontroller will give logic 0 and the time counter program will
run. //=====F1===== sensorFlow2 =
analogRead(A2); //sensor reading float Flow2 = sensorFlow2*5/1023;
if(Flow2<1&&kunci==1){ lcd.setCursor(17,1); lcd.print(":");
lcd.setCursor(15,1); lcd.print(menit); lcd.setCursor(18,1);
lcd.print(detik); wk2 = waktu2; kunci = 2; detik = 0; menit = 0; reset2 =
millis(); waktuFlow2 = wk2/3600; //s to h conversion formula fr2 =
1000/waktuFlow2; //flowrate formula v1 = v+1; if(vol = 2){ if(v1 == 1){
v1 = v1+1; vol = 1; digitalWrite(7, HIGH); //solenoid topen } }
digitalWrite(8, HIGH); //solenoid open
//=====F2===== } } sensorFlow3 =
analogRead(A3); //sensor reading float Flow3 = sensorFlow3*5/1023; In
this program, "sensorFlow2" is an infrared photodiode
if(Flow3<1&&kunci==2){ sensor that shows the results of the first
calibration. lcd.setCursor(17,2); "SensorFlow3" shows the results of the
second calibration, and lcd.print(":"); "sensorFlow4" shows the results of
the third calibration. The lcd.setCursor(15,2); output of these three
sensors will go to the comparator input and, lcd.print(menit); from the
comparator output will go to pins A2, A3, and A6 on Arduino. The results
of the acquisition of time on each sensor lcd.setCursor(18,2); then enter
into the flow velocity formula. lcd.print(detik); C. Measurement Result of
Infrared Photodiode Sensor at wk3 = waktu3; Comparator Output kunci =
3; The measurement of the infrared photodiode sensor is done detik = 0;
by measuring the comparator output (Table I). In this circuit, menit = 0;
there are 4 outputs obtained from the comparison of the input reset3 =
millis(); voltage from the sensor and the reference voltage. waktuFlow3 =
wk3/3600; //s to h conversion formula TABLE I. MEASUREMENT RESULT
OF INFRARED PHOTODIODE SENSOR fr3 = 1000/waktuFlow3; //flowrate
formula AT THE COMPARATOR OUTPUT if(vol = 1){ v1 = v1+1; Sensor Not
Blocked by Water Blocked by Water } 1 2.63 Volt 0.02 Volt if(v1 == 2){
vol = 2; 2 3.27 Volt 0.00 Volt } } 3 3.20 Volt 0.00 Volt
//=====F3===== sensorFlow4 =
analogRead(A6); //sensor reading 4 3.11 Volt 0.01 Volt float Flow4 =
sensorFlow4*5/1023; D. Measurement Result of Multiturn Resistance
if(Flow4<1&&kunci==3){ Multiturn resistance measurements are carried
out by lcd.setCursor(17,3); measuring the input pin and multiturn output
pin (Table II). lcd.print(":"); lcd.setCursor(15,3); TABLE II.
MEASUREMENT RESULT OF MULTITURN RESISTANCE lcd.print(menit);
lcd.setCursor(18,3); Multiturn Resistance (K $\Omega$ ) lcd.print(detik); 1 88.5
wk4 = waktu4; kunci = 4; 2 5.7 detik = 0; 3 13 menit = 0; if(timer==1){ 4
13.8 waktustart(); E. Measurement Result of Syringe Pump Using Infusion

```

} Device Analyzer timer = 0; Syringe pump performance measurement is done to reset4 = millis(); determine the performance of the Infusion Device Analyzer. waktuFlow4 = wk4/3600; //s to h conversion formula Syringe Pump performance data retrieval is done in 3 settings, fr4 = 1000/waktuFlow4; //flowrate formula namely 10 ml/hour as much as 1-time measurement, 50 ml/hour as much as two times the measurement, and 100 ml/hour as much as two times the measurement. Each measurement produces three calibration results (Table III). TABLE III. MEASUREMENT REASULT OF SYRINGE PUMP PERFORMANCE Set Flow Measurement Result (ml/h) I II III 10 ml/h 9.90 8.93 9.26 50 ml/h 50.00 43.48 47.62 47.62 43.48 47.62 100 ml/h 111.11 90.91 100.00 83.33 90.91 100.00 TABLE IV. THE AVERAGE AND ERROR MEASUREMENT OF THE SYRINGE PUMP ON FLOWRATE PARAMETERS No Flowrate (ml/h) Mean (ml/h) Error (%) 1 10 9.36 6.4 2 50 46.64 6.72 3 100 96.04 3.96

IV. DISCUSSION In this study, researchers measured the flow rate at the TOP- 5300 syringe pump. TABLE III shows that the measurements were carried out at a flow rate setting of 10 ml/hour with one- time data collection at a setting of 50 and 100 ml/hour with two times each data collection. TABLE IV shows the measurement results at the setting of 10 ml/hour yields an average of 9.36 ml/hour with an error value of 6.4%. At a setting of 50 ml/hour produces an average of 46.64 ml/hour with an error value of 6.72%, and at a setting of 100 ml/hour produces an average of 96.04 ml/hour with an error value of 3.96%. When referring to the measurement results on TABLE IV, this tool is said to be unfit for use because it has a high error value. However, the truth cannot be ascertained because the researcher did not compare the measurement results with standard measuring instruments. When compared with previous studies [4], with the use of the same sensor and system, this study experienced a decrease in the value of the resulting error. The decrease is the level of accuracy, and the precision of this device can be said to below, and it can be seen in TABLE IV. This can occur due to improper placement of sensors. The presence of air bubbles during the measurement process also affects the results of sensor readings. In addition, it is possible that the flow velocity generated by the motor on the syringe pump is unstable. In a practical system, this research can actually speed up the measurement time because this device can produce three calibration results in one measurement at the same flow rate setting. Although it can produce three calibration results, when referring to the measurement results on TABLE IV, this tool is said to be unfit for use because it has a high error value. However, the truth cannot be ascertained because the researcher did not compare the measurement results with standard measuring instruments.

V. CONCLUSION The purpose of the current study was to show the development of a flow rate calibrator that displays three calibration results in one measurement at the same setting. This research has found that a photodiode and infrared can be flow rate detectors. The study uses programming with Arduino Nano to create the desired system and is displayed on an LCD character 2004A. This study has an average error value of 5.69%, which means it exceeds the ECRI 416-0595 tolerance limit of $\pm 5\%$. In summary, the study unveils the device does not meet the standards and cannot be implemented as an infusion pump calibrator and syringe pump device. A further experimental investigation is needed to reduce the value of errors, improve systems and mechanics, display the results on LCD graphics, and increase storage.

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